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WO 01/15753 1 PCT/EP00/08157

# NEW HUMANIZED BIOMATERIALS, A PROCESS FOR THEIR PREPARATION AND THEIR APPLICATIONS

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The invention relates to new humanized biomaterials, a process for their preparation and their applications.

Tissue repair is needed after severe bone fractures, cartilage loss or general fragilization during ageing.

Artificial metallic or even ceramic prostheses are not very well integrated within host tissues and replacement with new surgery is often required after a few years, a major problem of handicap for old people.

Autologous grafts of bones or cartilage tissue is very difficult and costly. New technologies develop porous matrices implanted as scaffold prosthesis.

These matrices can eventually be filled with growth factors for the tissue regeneration or even with bone marrow stem cells.

However, fixation of cells or factors in the porous matrices with very prolonged and slow release of growth factors is very difficult to achieve and the ideal cocktail and concentration of factors required is unknown.

The aim of the present invention is to provide a homogeneous humanized, bioactive biomaterial (for example porous ceramics) that can be used for implantation purposes and which do not present the long term biocompatibility problems of prior art.

Another aim of the invention is to provide a bioactive biomaterial enabling tissue growth (for example bone and cartilage) in its porous space and securing the integration of the grafted biomaterial in the surrounding tissues (viable bones...).

Another aim of the invention is to provide long lasting prostheses, which avoids requirement for replacement of biomaterial prostheses after 10 years, as often needed up to now.

These aims are achieved by the invention, which consists in humanized biomaterial comprising a porous biocompatible composite material customized and implanted with monocyte derived cells and preferably with macrophages.

The expression "humanized" means that the porous biomaterial has been colonized with human cells derived from blood monocytes.

The expression "biocompatible composite" material designates a material composed of one or several of the following materials proved to be non toxic for human tissues (carbon microfibers, ceramics, calcium phosphates, metal oxides, collagen polymers...).

WO 01/15753 2 PCT/EP00/08157

The expression "porous" means that the biomaterial and preferably the ceramic present pores of about 100 to 2000 microns of diameter.

The expression "customized and implanted" material means that the shape and size of biomaterial is designed specifically for a patient and a site of implantation.

The expression "monocyte derived cells" corresponds to human mononuclear cells isolated from blood, enriched in monocytes and cultured at

37° C in appropriate medium, for 5 to 10 days to obtain tissue type macrophages.

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The monocyte derived cells used in the invention are for instance such as those described in PCT/EP 93/01232, WO 99/13054, EP 96/ 901848.0-2107, WO 97/44441.

In a particular embodiment of the invention, the monocyte derived cells described above, contain exogenous compounds such as drugs, proteins, growth factors of interest.

In another embodiment, the monocyte derived cells as described above contain in their cytoplasm exogenous DNA coding for a protein of interest.

The substantially irreversible humanization of matrices of biocompatible composite material described in the present invention allows a physiological interaction between the prostheses made of the biomedical composite, grafted and the host cells in the body. These relations with host tissue cells and with the extracellular matrix allow reconstruction of epithelial sheets and growth of a capillary network around the grafted biomaterial by local multiplication and sprouting of endothelial cells.

The monocyte derived cells, in particular the macrophages used to humanize *in vitro* the porous material in the invention are particularly adequate to increase integration and *in vivo* lifespan of biocompatible prostheses.

Advantageously, the humanized biomaterial of the invention is homogenous.

According to an advantageous embodiment, in the humanized biomaterial of the invention, the biocompatible composite material is chosen among the following materials: microfibres, ceramic materials, metal oxides such as aluminum oxide, calcium phosphate ceramic, glass or carbon fibers, hydroxylapatite, silicon carbide or nitride, collagen polymers or a mixture of these different materials.

According to another advantageous embodiment, in the humanized biomaterial of the invention, the human macrophages are liable to be obtained by ex vivo differentiation from blood monocytes leading to living macrophages, and are cultured under conditions enabling their penetration and adherence into the biomaterial for instance for several hours at 37°C, with the porous biomaterial, allowing infiltration of the biomaterial and substantially irreversible binding of the living macrophages to

the biomaterial, now humanized with patient's macrophages and ready for implantation.

The expression "substantially irreversible binding" means that macrophages are tightly bound by numerous contacts with the material and cannot be detached under physiological conditions.

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The invention also relates to a living body-supporting implant, characterized by the fact that it comprises or consists of the humanized biomaterial according to any one of claims 1 to 3, and is preferably structured under the form of scaffold, tissue-supporting sponges, bone or cartilage.

The expression "living body-supporting implant" designates an implant having for example the physical form and robustness of a bone to be replaced.

The expression "scaffold" designates a physical structure eventually metallic which keeps the biomaterial (ceramics or other) in the appropriate conformation.

The expression "tissue supporting sponges" designates a soft implant formed for instance of collagen which will be humanized with macrophages before insertion in the body.

The invention also relates to the use of a humanized biomaterial of the invention or of a living body-supporting implant of the invention, for the preparation of a tissue implant destined to replace or repair defective tissue, such as defective bone, cartilage, dental tissue, fibrous tissue, fibrocartilaginous supporting tissue.

The expression "fibrous tissue" designates tissues surrounding organs which support this organ and maintain the shape of this body part: they are mainly formed by epithelial sheets.

According to another advantageous embodiment, the invention relates to the use of a humanized biomaterial of the invention or of a living body-supporting implant of the invention, wherein the monocyte derived cells or macrophages are autologous with respect to the tissue to be replaced or repaired, enabling the biomaterial or the living body-supporting implant to be recognized as self.

The expression "implant to be recognized as self" means that it contains cells (i.e. macrophages) from the patient in which it will be grafted and is therefore autologous to the host.

A process for the preparation of a humanized biomaterial of the invention comprises the following steps:

- preparation of the porous biomaterial structured in form of bones, cartilage,
- preparation of macrophages from blood monocytes,

WO 01/15753 4 PCT/EP00/08157

- immersion of the biomaterial in a physiologic solution appropriate for the culture of macrophages which are added afterwards (ex. : phosphate buffered saline, medium such as RPMI, IMDM, AIMV),

- addition of the macrophage to the solution under conditions enabling binding to the biomaterial and particularly for 1 to 20 h. at 37°C, 5 % CO2 and 5 % air,
- washing of the biomaterial and conservation until use in physiologic medium.

A process for the preparation of a living body-supporting implant of the invention comprises the following steps:

- preparation of a customized porous implant or scaffold composed of bio-compatible material, according to any one of claims 1 to 3,
- preparation of macrophages from blood monocytes of the patient needing the customized implant of biomaterial,
- co-culture of macrophages and the implant in adequate medium under conditions enabling penetration and adherence to the biomaterial, in particular at 37°C, 5% CO2 in hydrophobic bags or containers until grafting the implant.

The invention also relates to the use of the humanized biomaterial or of a living body-supporting implant, which can be implanted in a tissue, for the *in vitro* or *in vivo* or *ex vivo* delivery of factors chosen in the group of chemokines and/or monokines, and/or cytokines and/or growth factors, the factors released being useful for the local attraction of cells required for tissue growth (such as osteoblasts, chondrocytes, fibroblasts, epithelial cells.....) and/or for the neovascularization around the implanted biomaterial, and/or for the release of growth factors sustaining proliferation of cells and/or the growth of new tissues.

Indeed, macrophages maintain tissue homeostasis through the secretion of at least 80 growth factors or monokines controlling and inducing proliferation of mesenchymal (fibroblasts....), endothelial, chondrocytes, osteoblasts, epithelial cells.. They also secrete enzymes and mediators allowing growth and renewal of the surrounding cells and tissues (see Table 1).

The key factors secreted by macrophages supporting tissue integration regeneration and growth of mesenchymal cells are: IGF1 and TGFs, but also PDGF, bFGF, MDGF, GM, CSF, NAF, IL-8, TNF, angiogenin and angiogenic factors. These growth factors allow also the development of all the steps required for angiogenesis, allowing neovascularisation and reconstitution of blood microcapillaries around the grafted biomaterial.

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In this aspect, macrophages are synthesizing 10 fold more proteins than monocytes, much more growth factors and less inflammatory mediators.

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#### TABLE 1:

# GROWTH FACTORS PROTEINS AND MEDIATORS SUPPORTING TISSUE HOMEOSTASICS SECRETED BY NATURE MACROPHAGES

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### **ENZYMES:**

# Lyzosymes

Neutral proteases

Plasminogen activator

Collagenase Elastase

Angiotensin-convertase

Acid hydrolases

Proteases Lipases Ribonucleases Phosphatases Glycosidases Sulphatases

Arginase

#### COMPLEMENT COMPONENTS

C1, 4, 2, 3 and 5

Factors B and D and Properdin

C1 inhibitor

C3b inactivator and  $\beta$ -1H

#### **ENZYME INHIBITORS**

(Antiproteases)

 $\alpha$ 1-antiprotease Plasmin inhibitors  $\alpha$ -2 macroglobulin

Plasminogen activator inhibitors

#### **PROTEINS BINDING**

**METABOLIOUS AND LIPIDS:** 

Acidic isoferritins

#### **BIOACTIVE LIPIDS:**

Arachidonic acid metabolites

Prostaglandins E2, F2α

Prostacyclin Thromboxane

Leukotrienes B4, C, D and E Hydroxy-eicosatetraneoic acids

(including SRS-A)
Platelet activating factors

## CYTOKINES, HORMONES,

#### **GROWTH FACTORS:**

Interleukins 1  $\alpha$  and  $\beta$ Tumours necrosis factor  $\alpha$ Interferons  $\alpha$  and  $\beta_1$ , & Interleukin 6, 8, 13, 18 Chemotatic factors for

Neutrophils Tlymphocytes Monocytes Fibroblasts

Heamatopoceitic Colony Stimulating

Factors for

Granulocyte-Macrophages (GM-CSF)

Granulocytes (G-CSF)
Macrophages (M-CSF)

Erythropoeitin Growth factors

Fibroblasts growth factor /

Insuline like G.F.

"platgelet-derived growth factor"

(PDGF)

Transforming growth factor  $\alpha$  and  $\beta$ 

Endothelial cell growth factor

Hormones

 $1 \alpha$ , 25-Dihydroxyvitamin D3

Transferrin
Transcobalamin II
Fibronectin
Laminin
Lipid transfer protein
Thrombospondin

NUCLEOSIDES AND
METABOLITES:
Thymidine and deoxycytidine
Uracil
Uric acid
Lactic acid
Polyamines nitrines and nitrates
Neopterin

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Insulin-like activity, protagandins
Thymosin B4
β endorphin
Adrenocorticotrophic hormone

CHEMOKINES MIP / RANTE FAMILIES COAGULATION FACTORS: Factors III, VIII, and tissue factor Prothrombin and prothrombinase Factors IX, X, V and VII

In an advantageous embodiment of the invention, the macrophages migrate initially in the porous biomaterial and incorporate irreversibly into this prosthesis by very strong adherence and spreading. When they are kept in physiological conditions, macrophages are very long living cells lasting from several months to several years after implantation. During this time, macrophages will continuously secrete growth factors and cytokines in their local environment; these factors will act in synergy at very low concentrations (10 <sup>-10</sup> M) on the surrounding cells and tissues.

Furthermore, macrophages do present on their membranes receptors for cytokines, hormones, sugars allowing to respond to micro-environmental needs and to adjust their secretion to the local status around the biomaterial at different periods after grafting.

The growth factors secreted by macrophages represent the global requirements for tissue repair, differentiation and local angiogenesis. The chemokines which will be continuously released in a concentration gradient around the implant will call in and around the prosthesis cells required for recolonization and integration of the biomaterial in host environment. Therefore, the new customized porous biomaterials colonized with host macrophages present a novel biotolerance and a length of adequate performance far better than prosthesis used in the absence of autologous macrophages. Applications are very large in solid or cartilaginous prosthesis needed in bone, cartilaginous repair particularly.

According to another advantageous embodiment, the invention relates to the use of the humanized biomaterial or of a living body-supporting implant, as a graft for the replacement of supporting tissues such as bones, cartilages, dental tissues, epithelial sheet and subcutaneous tissue matrix.

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#### Example 1:

A calcium phosphate porous ceramic with pores of 200 to 2000 microns (porosity > 20 % and < 80 %) is placed on an hydrophobic support (ethylene vinyl acetate) in the presence of 50 ml AIMV culture medium (life-cell Gibco, Paisley G.B.). Macrophages are added to this preparation at the concentration of 5.10<sup>6</sup> cells/ml; they are obtained after 7 days differentiation of blood monocytes in culture according to published state of the art in publications and patents (PCT/EP 93/01232, WO 99/13054, EP 96/ 901848.0-2107, WO 97/44441); a control preparation is maintained in the absence of macrophages. The preparation is incubated overnight at 37 °C, 5 % CO2, 95 % air to allow fixation of macrophages on the ceramic.

The porous ceramic is washed and cultured in the presence of fibroblasts and/or in the presence of chondrocytes In both cases, the cell proliferation is higher by a factor 2 to 10 for the porous ceramic colonized with macrophages, compared to control ceramic.

#### Example 2:

A small fragment of porous microceramic is implanted in a rabbit cornea. The inert microceramic piece induces a very small to moderate inflammation and only peripheral growth of new blood vessels from the ring of the cornea.

In contrast, microceramic covered with macrophages, as described in example 1 induces a major neovascularisation towards the center of the cornea. The cornea becomes vascularized through an invasion of endothelial cells arising from the rim rich in blood supply and sprouting towards the biomaterial implanted.

#### Example 3:

Fragments of 100 +/- 20 mg of hydroxyapatite ceramic (Endobon®, Merck) and pieces of one cm2 of a polypropylene scaffold are prepared. Fresh non activated macrophages obtained after 7 days differentiation of blood monocytes in culture according to published patent applications (WO94/26875, WO 99/13054, WO96/22781, WO 97/44441) are suspended (2,5.106 cells/ml) in IMDM (Iscove Modified Dulbecco Medium) culture medium. Each biomaterial fragment is incubated in 1 ml of macrophage suspension, in sterile polypropylene tubes, for 4 hours at room temperature. To check the binding of macrophages on the biomaterial, cells present in the supernatant after incubation are counted. After incubation with Endobon®, from 12 to 17% of the cells added were present in the supernatant (3 experiments),

WO 01/15753 8 PCT/EP00/08157

indicating that more than 2.10<sup>6</sup> macrophages are adsorbed on 100 mg of porous ceramic. After incubation with polypropylene scaffold, from 23 to 55 % of the cells initially added are present in the supernatant, indicating adsorption of 1 to 2.10<sup>6</sup> macrophages/cm2 scaffold.

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Nude mice are implanted with biomaterial, and each mouse receives two implants of the same type, one in each flank.

Mice n°	Implanted material
1, 2	Endobon® colonized by macrophages
3	Endobon®
4, 5	Polypropylene colonized by macrophages
6	Polypropylene

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Mice are sacrificed after 21 days, macroscopic observation shows no major difference between implants of biomaterial alone and implants of biomaterial colonized by macrophages.

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Microscopic observation of tissues in paraffin shows that, when compared to implants of biomaterial alone, implants of biomaterial colonized by macrophages induce first an inflammation phenomenon, which is an important step to induce migration and homing of competent cells for tissue repair. A more important neovascularisation at the implantation site of biomaterial colonized with macrophages has also been observed.

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The histological analysis of tissues in resin confirms the increase of neovascularisation for mice implanted with macrophages colonized biomaterials; when compared to mice implanted only with biomaterial.

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The therapeutic applications for tissue repair are confirmed in human bearing non healing ulcers. The ulcers covered with scaffold implanted with autologous macrophages show an improved cicatrization as measured by detersion and size of the ulcer.

## **CLAIMS**

- 5 1 Humanized biomaterial comprising a porous biocompatible composite material customized and implanted with monocyte derived cells and preferably with macrophages.
  - 2 Humanized biomaterial according to claim 1, wherein the biocompatible composite material is chosen among the following materials: microfibers, ceramic materials, metal oxides such as aluminum oxide, calcium phosphate ceramic, glass or carbon fibers, hydroxylapatite, silicon carbide or nitride, collagen polymers or a mixture of these different materials.

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- 15 3 Humanized biomaterial according to claims 1 or 2, wherein the human macrophages are liable to be obtained by ex vivo differentiation from blood monocytes leading to living macrophages, and are cultured under conditions enabling their penetration and adherence into the biomaterial, for instance for several hours at 37°C, with the porous biomaterial, allowing infiltration of the biomaterial and substantially irreversible binding of the living macrophages to the biomaterial, being humanized with patient's macrophages and ready for implantation.
  - 4 Living body-supporting implant, characterized by the fact that it comprises or consists of the humanized biomaterial according to any one of claims 1 to 3, and is preferably structured under the form of scaffold, tissue-supporting sponges, bone or cartilage.
  - 5 Use of a humanized biomaterial according to any one claims 1 to 3 or of a living body-supporting implant according to claim 4, for the preparation of a tissue implant destined to replace or repair defective tissue, such as defective bone, cartilage, dental tissue, fibrous tissue, fibrocartilaginous supporting tissue.
  - 6 Use of a humanized biomaterial according to any one of claims 1 to 3 or of a living body-supporting implant according to claim 4, wherein the monocyte derived cells or macrophages are autologous with respect to the tissue to be replaced or repaired, enabling the biomaterial or the living body-supporting implant to be recognized as self.

WO 01/15753 10 PCT/EP00/08157

- 7 Process for the preparation of a humanized biomaterial according to any one claims 1 to 3, comprising the following steps:
  - preparation of the porous biomaterial structured in form of bones, cartilage,
  - preparation of macrophages from blood monocytes,
  - immersion of the biomaterial in a physiologic solution appropriate for the culture of macrophages which are added afterwards (ex. : phosphate buffered saline, medium such as RPMI, IMDM, AIMV),
  - addition of the macrophages to the solution under conditions enabling binding to biomaterial and particularly for 1 to 20 h. at 37°C,
    - 5 % CO2 and 5 % air,

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- washing of the biomaterial and conservation until use in physiologic medium.
- 8 Process for the preparation of a living body-supporting implant according to claim 4, comprising the following steps:
  - preparation of a customized porous implant or scaffold composed of bio-compatible material, according to any one of claims 1 to 3,
  - preparation of macrophages from blood monocytes of the patient needing the customized implant of biomaterial,
  - co-culture of macrophages and the implant in adequate medium under conditions enabling penetration and adherence to the biomaterial in particular at 37°C, 5% CO2 in hydrophobic bags or containers until grafting the implant.
- 9 Use of the humanized biomaterial according to any one of claims 1 to 3 or of a living body-supporting implant according to claim 4, which can be implanted in a tissue, for the *in vitro* or *in vivo* or *ex vivo* delivery of factors chosen in the group of chemokines and/or monokines, and/or cytokines and/or growth factors, the factors released being useful for the local attraction of cells required for tissue growth (such as osteoblasts, chondrocytes, fibroblasts, epithelial cells.....) and/or for the neovascularization around the implanted biomaterial, and/or for the release of growth factors sustaining proliferation of cells and/or the growth of new tissues.

10 - Use of the humanized biomaterial according to any one of claims 1 to 3 or of a living body-supporting implant according to claim 4, as a graft for the replacement of supporting tissues such as bones, cartilages, dental tissues, epithelial sheet and subcutaneous tissue matrix.

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A. CLASS IPC 7	A61L27/40 A61L27/38			
	to International Patent Classification (IPC) or to both national classifi	cation and IPC		
	SEARCHED  ocumentation searched (classification system followed by classification system followed by classif	tion symbole)		
IPC 7	A61L	ion symbols)		
Documenta	tion searched other than minimum documentation to the extent that	such documents are include	d in the fields s	earched
Electronic o	lata base consulted during the international search (name of data ba	ase and, where practical, se	arch terms use	i)
	ternal, WPI Data, PAJ			
C. DOCUM	ENTS CONSIDERED TO BE RELEVANT			
Category °	Citation of document, with Indication, where appropriate, of the rel	evant passages		Relevant to claim No.
X	US 5 902 741 A (DUNKELMAN NOUSHIN 11 May 1999 (1999-05-11) abstract	ET AL)		1,2,4-10
	column 8, line 59 -column 9, line column 10, line 63 -column 11, li column 13, line 12 - line 40	: 57 ne 9		
X	US 5 885 829 A (RUTHERFORD ROBERT AL) 23 March 1999 (1999-03-23) column 3, line 64 -column 4, line column 5, line 56 -column 6, line column 11, line 16 - line 65 column 13, line 20 - line 67	31		1,2,4-10
x	DE 38 10 803 A (BATTELLE INSTITUT 12 October 1989 (1989-10-12) column 1, line 25 -column 2, line column 2, line 67 -column 3, line	13		1-5,7-10
X Furthe	er documents are listed in the continuation of box C.	X Patent family memb	ers are listed in	annex.
"A" document conside "E" earlier do filing da "L" document which is citation	raderining the general state of the art which is not red to be of particular relevance current but published on or after the international te.  It which may throw doubts on priority claim(s) or cited to establish the publication date of another or other special reason (as specified)  It referring to an oral disclosure, use, exhibition or	I' later document published or priority date and not is cited to understand the priority of the cannot be considered not involve an inventive step of document of particular recannot be considered not particular particular processing the cannot be considered to document is combined with the considered to	evance; the cla evance; the cla evel or cannot b when the docu evance; the cla involve an inve	le application but ry underlying the  Imed invention e considered to ment is taken alone imed invention ntive step when the other sub drow
later tha		ments, such combination in the art.  document member of the		
	tual completion of the international search	Date of mailing of the into	ernational searc	th report
	November 2000	05/12/2000		
ramo anu Ma	illing address of the ISA European Patent Office, P.B. 5818 Patentiaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Tx. 31 651 epo ni, Fax: (+31-70) 340-3016	Authorized officer  Menidjel, F	₹	

Intern nal Application No
PCT/EP 00/08157

		PCT/EP 00/08157			
(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT					
Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.			
<b>(</b>	US 4 485 096 A (BELL EUGENE) 27 November 1984 (1984-11-27) column 1, line 37 -column 2, line 6 column 2, line 67 -column 3, line 64 column 4, line 31 - line 54	1,2,4~8			
	EP 0 798 374 A (MATRIX MEDICAL B V) 1 October 1997 (1997-10-01) column 2, line 6 -column 3, line 31	1,2,4-8			

information on patent family members

Interi nal Application No
PCT/EP 00/08157

Patent documer cited in search rep		Publication date		Patent family member(s)	Publication date
US 5902741	A	11-05-1999	US	5443950 A	22-08-1995
	,,	00 1333	US	5266480 A	30-11-1993
			US	5032508 A	16-07-1991
			US	4963489 A	
			US		16-10-1990
				4721096 A	26-01-1988
			AU	689605 B	02-04-1998
			AU	2769695 A	04-01-1996
			CA	2192064 A	14-12-1995
			EP	0812351 A	17-12-1997
			NZ	288467 A	28-10-1998
•			WO	9533821 A	14-12-1995
			US	5962325 A	05-10-1999
			US	6140039 A	31-10-2000
			US	6022743 A	08-02-2000
	•		US	5863531 A	26-01-1999
			US	5460939 A	24-10-1995
			US	5510254 A	23-04-1996
			US	5580781 A	03-12-1996
			US	5516680 A	14-05-1996
			ÜS	5512475 A	30-04-1996
			ÜS	5541107 A	30-07-1996
			US	5516681 A	14-05-1996
			US	5578485 A	26-11-1996
			US	5785964 A	28-07-1998
			US	5518915 A	21-05-1996
			US	5624840 A	
			US		29-04-1997
				5849588 A	15-12-1998
			US	5858721 A	12-01-1999
			AU	644578 B	16-12-1993
			AU	4211489 A	02-04-1990
			BR	8907642 A	20-08-1991
			CA	1335657 A	23-05-1995
			DK	40591 A	07-05-1991
			EP	0358506 A	14-03-1990
			HU	56393 A	28-08-1991
			ΙĻ	91536 A	31-10-1996
			JP	4501657 T	26-03-1992
		:	KR	156571 B	15-10-1998
			KR	156684 B	15-10-1998
			KR	156685 B	15-10-1998
			NO	910787 A	22-04-1991
			NZ	230572 A	23-12-1993
			PT	91676 A	30-03-1990
			WO	9002796 A	22-03-1990
			US	5160490 A	03-11-1992
			ZA	8906886 A	27-06-1990
			AT	127692 T	15-09-1995
			AU	6815990 A	
ويود وي دي ديد اها ها اها اها اها اها اها اها اها اها			AU	0019330 H	14-03-1991
US 5885829	Α	23-03-1999	AU	3214797 A	05-01-1998
			EP	0915967 A	19-05-1999
			WO	9745533 A	04-12-1997
DE 3810803	A	12-10-1989	NONE		
US 4485096	Α	27-11-1984	AT	25193 T	15-02-1987
			DE	3369465 D	05-03-1987
			EP	0110966 A	20-06-1984

## FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

Continuation of Box I.1

Although claims 1,9 are directed to a method of treatment of the human/animal body, the search has been carried out and based on the alleged effects of the compound/composition.

Continuation of Box I.1

Rule 39.1(iv) PCT - Method for treatment of the human or animal body by therapy

information on patent family members

Inten nal Application No PCT/EP 00/08157

Patent document cited in search report	-	Publication date		Patent family member(s)	Publication date
US 4485096	A		WO US	8304177 A 4485097 A	08-12-1983 27-11-1984
EP 0798374	A	01-10-1997	CA	2198978 A	01-09-1997

Form PCT/ISA/210 (patent family annex) (July 1992)